



Special article

Physiological impact of the facial mask at rest (2): Modification of Cardiac Variability (HRV) in young athletes

Ignasi de Yzaguirre Maura^{a,*}, Jaume Escoda i Mora^a, Mauricio Monaco^b, Gonzalo Grazioli^c, Jordi Santiago^a, Daniel Brotons i Cuixart^a

^a Unitat d'Esport i Salut, Generalitat of Catalunya, (Esplugues de Llobregat), 08950 Barcelona, Spain

^b Aspetar Orthopedic and Sports Medicine Hospital, Qatar

^c Aptima Center Clínic, Mutua Terrassa, Spain

ARTICLE INFO

Keywords:

Hypoxia

Hypercapnia

Rarefied air

Facial mask

Heart rate variability (HRV)

ABSTRACT

Introduction: During the imperative mandate of mask-wearing during the COVID-19 pandemic, our study aimed to elucidate the physiological repercussions stemming from hypoxia and hypercapnia induced by facemasks during periods of rest. Specifically, we investigated the influence of facemasks on heart rate variability (HRV) within a cohort of young athletes.

Material and methods: Experimental study in which 56 competitive adolescent athletes (55 % female) were evaluated. The heart rate data was recorded during 8-min, in meditative rest while seated. We conducted a comprehensive analysis of heart rate variability, examining both a 4-min segment and a 100-beat window. Comparisons were made between data recorded when subjects wore facemasks and when they breathed freely without masks. Data analysis was performed utilizing the Polar ProTrainer 5 software.

Results: The results showed relevant statistical differences at the level of cardiac variability (HRV): a) Heart Rate (mask: 70.5 ± 11.3 bpm vs no mask: 71.4 ± 12 bpm; $p < 0.043$. b) RMSSD (Mask: 56.8 ± 41.1 ms vs no mask: 48.9 ± 30.8 ms $p < 0.002$). c) RMSSD only 100 beats (mask: 58.1 ± 42.0 ms vs no mask: 46.7 ± 28.4 ms; $p < 0.0001$).

Conclusions: Upon removing the facemask while maintaining meditative rest, 86 % of the subjects exhibited a distinct sympathetic response during the subsequent 5-min period. Notably, in 13 % of participants, this sympathetic response persisted across both phases of the study. Furthermore, the analysis of Ultra-Short-Term Cardiac Variability based on 100 beats accentuated the significance of the observed differences.

Introduction

The aim of this study is to replicate the findings published, regarding the modifications in Cardiac Variability induced by the use of facemasks for COVID-19 prevention, as detected through routine electrocardiograms, during the annual sports medicine screening.¹ This work significantly increases the subject pool and incorporates a resting scenario to

enable the investigation of Cardiac Variability under both masked and unmasked conditions. These findings add to the studies of the impact of hypercapnic hypoxia and rarefied air in various situations carried out, since 2008.²⁻⁶

Study carried out without scholarships or financial budget. Original content, which has not been presented at any public event. The current study was carried out in the Metropolitan Area of Barcelona (Spain), in the physiology laboratory of the Sports and Health Unit of the General Secretariat of Sports (Government of Catalonia). The study took place in the Barcelona Metropolitan Area, during the COVID-19 pandemic (between 3/8/2021 to 6/15/2022). The laboratory air composition was: O₂: 20.9 % and CO₂: 578 ± 76 ppm. Our procedures complied with ethical guidelines from the Responsible Committee for Human Experimentation at Consell Català de l'Esport and with the principles of the 1975 Helsinki declaration. We extend gratitude to the Sports and Health Unit of the Government of Catalonia and the young athletes and families at the Blume Residence in Esplugues de Llobregat (Barcelona) for their consent and collaboration. The study has been favorably reported by the ethics committee of the sports administration of Catalonia (certificate: 018 / CEICGC / 2021).

* Corresponding author.

E-mail address: 14521iym@comb.cat (I. de Yzaguirre Maura).

<https://doi.org/10.1016/j.apunsm.2024.100472>

Received 7 October 2024; Accepted 24 November 2024

Available online 9 January 2025

2666-5069/© 2024 Published by Elsevier España, S.L.U. on behalf of Consell Català de l'Esport. This is an open access article under the CC BY-NC-ND license (<http://creativecommons.org/licenses/by-nc-nd/4.0/>).

Material and method

We assessed 56 adolescent athletes (55 % female) including 9 who had recovered from COVID-19 and were in good athletic shape, as can be seen in Table 1. We measured their heartbeats in milliseconds using a Polar S800i heart rate monitor during an 8-min session of relaxation with soothing music while sitting.⁷ Participants wore Type IIR face-masks (model NM12458) adjusted with a post-cervical tensioner. We conducted a double analysis of heart variability (HRV) for 4 min and 100 beats, comparing results with and without masks. Data were analyzed using Polar ProTrainer5 software, prioritizing robust scientific knowledge on cardiac variability.^{8–10}

Statistical study

Continuous variables were presented as means and standard deviations. A paired two-tailed T-test was employed to assess the significance of differences observed. When comparing the "men" and "women" groups, the variance of each group was determined due to the unpaired nature of the data, ensuring appropriate adjustment of the T-test.

The primary variables under scrutiny encompassed heart rate (HR) and the square root of the mean of the squares of the successive differences between adjacent normal beats (RMSSD).¹⁰

Results

In relation to cardiac variability (HRV), an analysis of 4 min of cardiac recording unveiled significant findings. Key parameters are as follows:

1. Heart rate exhibited a statistically significant increase upon subjects' removal of face masks: Heart Rate (mask: 70.5 ± 11.3 bpm vs no mask: 71.4 ± 12 bpm).
2. The square root of the mean of the squares of the successive differences between adjacent normal beats witnessed a highly significant decrease upon releasing subjects from face masks: RMSSD (Mask: 56.8 ± 41.1 ms vs no mask: 48.9 ± 30.8 ms).

Additional HRV parameters derived from the 4-min analysis are outlined below, as can be seen in Table 2, Table 3 and Table 4:

- a) The Relaxation index analyzed using Polar (RLX), expressed in milliseconds, showcased a notable decrease upon subjects' mask removal (Mask: 36.1 ± 21.7 ms vs no mask: 31.4 ± 16.6 ms).
- b) The width of the ellipse in the Poincaré diagram (SD1) exhibited a significant decrease when subjects were unmasked (Mask: 40.2 ± 29.1 ms vs no mask: 34.6 ± 21.8 ms).
- c) The percentage of normal, successive heartbeats with a difference greater than 50 milliseconds (pNN50) demonstrated a significant decrease upon mask removal (Mask: 13.2 ± 10.9 % vs no mask: 11.2 ± 9.6 %).
- d) Analysis in the frequency domain revealed a significant decrease in the high-frequency band (HF) upon subjects' mask removal (Mask: 1826 ± 2615 Hz vs no mask: 1339 ± 1580 Hz).

Upon conducting data analysis solely with 100 beats, both with and

Table 1
Physiological profile of study participants.

	Man	women	p<
Age (years)	18.5 ± 5.9	15.2 ± 2.35	0.02
Weight (Kg)	64.4 ± 8.6	57.6 ± 10.2	0.01
Height (m)	1.752 ± 0.09	1.70 ± 0.08	N.S.
BMI	20.9 ± 1.73	19.6 ± 2.23	0.02

BMI: Body Mass Index.

Table 2

Heart rate variability results. Total number of subjects studied, men and women.

Total: (Women + Men) n: 56	mask Average	Without Mask Average	p<
Minimum RR interval (ms)	711.2 ± 106	712.5 ± 141	N/S
Mean RR interval (ms)	874.2 ± 151.5	865.8 ± 158.1	N/S
Maximum RR interval (ms)	1088 ± 266.6	1068 ± 205	N/S
RLX baseline	36.1 ± 21.7	31.4 ± 16.6	0.009
SDNN (ms)	69.7 ± 33.9	68.1 ± 34.5	N/S
max/min ratio	1.5 ± 0.3	1.5 ± 0.3	N/S
RR weighted average (ms)	880.6 ± 153.7	872.3 ± 159.8	N/S
SD1	40.2 ± 29.1	34.6 ± 21.8	0.002
SD2	88.1 ± 39.6	88.8 ± 44.7	N/S
RMSSD (ms)	56.8 ± 41.1	48.9 ± 30.8	0.002
pNN50 (%)	13.2 ± 10.9	11.2 ± 9.6	0.002
SD2/SD1	2.6 ± 1	2.9 ± 0.9	0.013
Total power (0.003–0.400 Hz)	7544 ± 9577	6359 ± 6459	N/S
VLF (0.003–0.040 Hz)	3397 ± 6146	2818 ± 2569	N/S
LF (0.040–0.150 Hz)	2321 ± 3532	2203 ± 3123	N/S
HF (0.150–0.400 Hz)	1826 ± 2615	1339 ± 1580	0.018
LF/HF ratio	218.1 ± 214.7	238 ± 199	N/S
HR	70.5 ± 11.3	71.4 ± 12	0.043
HRV ultrashort (100 beats)			
amplitude 100 (ms)	331.8 ± 126	314.5 ± 118.9	N/S
mode 100 (%)	36.3 ± 14.6	38.3 ± 13.6	N/S
SD1 100	40.3 ± 29.9	32.9 ± 20.2	0.0003
SD2 100	82.6 ± 41.1	80.7 ± 40.6	N/S
SD2/SD1 100	2.44 ± 1.0	2.77 ± 0.9	0.0022
RMSSD 100 (ms)	58.1 ± 42.0	46.7 ± 28.4	0.0001

RLX baseline: Relaxation rate analyzed using Polar^R (RLX), expressed in milliseconds. **SDNN** (ms): standard deviation of "n" normal intervals. **SD1:** The width of the ellipse in the Poincaré diagram, relative to successive "rr". **SD2:** Length of the ellipse in the Poincaré diagram. **RMSSD** (ms): The square root of the mean of the squares of the successive differences between adjacent normal beats. **pNN50** (%): the proportion of normal and successive rr intervals, greater than 50 milliseconds, divided by total number of intervals. **Total power** (0.003–0.400 Hz): **VLF** (0.003–0.040 Hz): the very low frequency (VLF) from 0.0033 to 0.04 Hz. **LF** (0.040–0.150 Hz): **HF** (0.150–0.400 Hz): high frequency from 0.15 to 0.4 Hz. **HR:** heartbeat frequency. **HRV ultrashort (100 beats):** Cardiac variability performed with 100 successive beats. **Amplitude 100** (ms): Amplitude of the normal curve made with 100 successive beats. **Mode 100** (%): Statistical mode of the normal curve made with 100 successive beats, expressed in percentage.

without masks, the results exhibited even greater statistical significance:

- a) SD1 only 100 beats (mask: 40.3 ± 29.9 ms vs no mask: 32.9 ± 20.2 ms; $p < 0.0003$).
- b) SD2/SD1 only 100 beats (mask: 2.44 ± 1.0 ratio vs no mask: 2.77 ± 0.9 ratio; $p < 0.0022$).
- c) RMSSD only 100 beats (mask: 58.1 ± 42.0 ms vs no mask: 46.7 ± 28.4 ms; $p < 0.0001$).

Discussion

In our previous investigation,¹ we elucidated the effect of mask usage on the neurovegetative equilibrium of the participants, resulting in an increased predominance of the parasympathetic component.

That initial study was conducted utilizing standard 10-s electrocardiograms (ECG) obtained while the subjects wore mandatory masks during the pandemic and was retrospectively compared with ECG data collected in the previous year.

The current study aimed to validate the results of the prior investigation by expanding the sampling duration of heart rate data to 4 min, both with the subject wearing a mask and breathing freely without a mask while at rest.

Likewise, the statistical analysis was replicated using series of 100 heartbeats to assess the efficacy of this "ultrashort" method, as well as various *sphygmometry* techniques (histogram of heart rate distribution

Table 3
Heart rate variability results. Women only.

Women n: 31	Mask Average	Without Mask Average	p<
Minimum RR interval (ms)	681.9 ± 93	681.9 ± 102.8	N/S
Mean RR interval (ms)	838.2 ± 119	834.3 ± 118.3	N/S
Maximum RR interval (ms)	1060 ± 264	1019.6 ± 152.6	N/S
RLX baseline	33.7 ± 18.4	31.2 ± 15	N/S
SDNN (ms)	69.3 ± 34.4	64.9 ± 32.8	N/S
max/min ratio	1.6 ± 0.3	1.5 ± 0.2	N/S
RR weighted average (ms)	845 ± 122	841.2 ± 120	N/S
SD1	39.6 ± 30.8	34.2 ± 21.5	0.045
SD2	87.3 ± 39.2	91.1 ± 42	N/S
RMSSD (ms)	56.1 ± 43.5	48.4 ± 30.5	0.045
pNN50 (%)	12.1 ± 10.5	10.7 ± 9.3	N/S
SD2/SD1	2.6 ± 0.8	2.9 ± 0.8	0.015
Total power (0.003–0.400 Hz)	8254 ± 11550	6337 ± 6467	N/S
VLF (0.003–0.040 Hz)	41001 ± 8160	2680.6 ± 2288	N/S
LF (0.040–0.150 Hz)	2154 ± 3614	2216.1 ± 3417	N/S
HF (0.150–0.400 Hz)	2000 ± 3088	1441.2 ± 1770	N/S
LF/HF ratio	167 ± 140	207.7 ± 176.7	N/S
HR	72.9 ± 9.9	73.3 ± 9.9	N/S
HRV ultrashort (100 beats)			
amplitude 100 (ms)	315.5 ± 121.1	300 ± 101	N/S
mode 100 (%)	37.9 ± 15	36.5 ± 11.9	N/S
SD1 100	38.1 ± 30.8	32 ± 19.1	0.044
SD2 100	79.2 ± 43.6	79.6 ± 38.9	N/S
SD2/SD1 100	2.3 ± 0.8	2.7 ± 0.8	0.020
RMSSD 100 (ms)	55.6 ± 44.3	46 ± 27.3	0.030

RLX baseline: Relaxation rate analyzed using Polar^R (RLX), expressed in milliseconds. **SDNN (ms):** standard deviation of "n" normal intervals. **SD1:** The width of the ellipse in the Poincaré diagram, relative to successive "rr". **SD2:** Length of the ellipse in the Poincaré diagram. **RMSSD (ms):** The square root of the mean of the squares of the successive differences between adjacent normal beats. **pNN50 (%):** the proportion of normal and successive rr intervals, greater than 50 milliseconds, divided by total number of intervals. **Total power (0.003–0.400 Hz):** **VLF (0.003–0.040 Hz):** the very low frequency (VLF) from 0.0033 to 0.04 Hz. **LF (0.040–0.150 Hz):** **HF (0.150–0.400 Hz):** high frequency from 0.15 to 0.4 Hz. **HR:** heartbeat frequency. **HRV ultrashort (100 beats):** Cardiac variability performed with 100 successive beats. **Amplitude 100 (ms):** Amplitude of the normal curve made with 100 successive beats. **Mode 100 (%):** Statistical mode of the normal curve made with 100 successive beats, expressed in percentage.

with a 50 ms range) advocated by S. Tjfvinski¹⁵ in 1991. Additionally, the *correlational rhythmogram* (also known as Scaterogram, Poincaré diagram...) proposed by E. Zemtsovski et al. in 1977 was employed.¹⁶

Our findings elucidate the degree to which cardiac variability predominantly emerges as an adaptive reaction to subtle hypoxic and hypercapnic circumstances induced by the utilization of infection prevention masks. This adaptation demonstrates statistical significance across all pivotal variables scrutinized in our study, notably heart rate (HR) and the analysis of the interval between successive beats (RMSSD). Our results are consistent with the ultrashort methodologies advocated by Nunan et al.¹¹

Contributions of our research reaffirm the conclusions drawn by our team regarding the impact of masks on neurovegetative balance.¹ Furthermore moreover, it validates the efficacy and sensitivity of ultrashort methodologies in assessing heart rate variability (HRV),^{11–13} particularly the traditional 100-beat method.

Limitations of our study: In our investigation, the cohort consisting of "n = 31" women had lower values for the primary parameters investigated: heart rate and RMSSD, in comparison to their male counterparts. However, it is noteworthy that the female participants were from a younger age group relative to the male cohort.

We attribute the observed discrepancy in adaptation to anatomical distinctions between the male and female subjects, rather than age-related effects. Specifically, it is acknowledged that individuals with greater stature typically possess a larger anatomical dead space.

Table 4
Heart rate variability results. Men only.

Men n = 25	Mask Average	Without Mask Average	p<
Minimum RR interval (ms)	744 ± 111.7	747 ± 169.8	N/S
Mean RR interval (ms)	914.3 ± 174.4	901.0 ± 189.5	N/S
Maximum RR interval (ms)	1119 ± 271	1117.3 ± 243.1	N/S
RLX baseline	38.8 ± 25	31.5 ± 18.5	0.024
SDNN (ms)	70.2 ± 34	66.7 ± 37	N/S
max/min ratio	1.5 ± 0.3	1.5 ± 0.4	N/S
RR weighted average (ms)	920.3 ± 177.3	907.0 ± 102	N/S
SD1	40.7 ± 20.7	35.0 ± 22.5	0.017
SD2	88.9 ± 40.8	86.2 ± 48.2	N/S
RMSSD (ms)	57.6 ± 35.1	49.5 ± 31.8	0.017
pNN50 (%)	14.4 ± 11.5	11.7 ± 10	0.009
SD2/SD1	2.7 ± 1.2	2.8 ± 1	N/S
Total power (0.003–0.400 Hz)	6751 ± 6888	6383 ± 6578	N/S
VLF (0.003–0.040 Hz)	2611 ± 2409	2971 ± 2888	N/S
LF (0.040–0.150 Hz)	2507 ± 3500	2188 ± 2826	N/S
HF (0.150–0.400 Hz)	1633 ± 2005	1225 ± 1364	N/S
LF/HF ratio	275 ± 267	271 ± 220	N/S
HR	67.8 ± 12.3	69.3 ± 13.9	0.047
HRV ultrashort (100 beats)			
amplitude 100 (ms)	350 ± 131	331 ± 136	N/S
mode 100 (%)	34.5 ± 14.2	40.2 ± 15.4	0.0006
SD1 100	43 ± 29	33.9 ± 22	0.0011
SD2 100	85.9 ± 38.9	82.0 ± 43.1	N/S
SD2/SD1 100	2.5 ± 1.2	2.8 ± 1.0	N/S
RMSSD 100 (ms)	60.8 ± 39.9	47.4 ± 30.1	0.0004

RLX baseline: Relaxation rate analyzed using Polar^R (RLX), expressed in milliseconds. **SDNN (ms):** standard deviation of "n" normal intervals. **SD1:** The width of the ellipse in the Poincaré diagram, relative to successive "rr". **SD2:** Length of the ellipse in the Poincaré diagram. **RMSSD (ms):** The square root of the mean of the squares of the successive differences between adjacent normal beats. **pNN50 (%):** the proportion of normal and successive rr intervals, greater than 50 milliseconds, divided by total number of intervals. **Total power (0.003–0.400 Hz):** **VLF (0.003–0.040 Hz):** the very low frequency (VLF) from 0.0033 to 0.04 Hz. **LF (0.040–0.150 Hz):** **HF (0.150–0.400 Hz):** high frequency from 0.15 to 0.4 Hz. **HR:** heartbeat frequency. **HRV ultrashort (100 beats):** Cardiac variability performed with 100 successive beats. **Amplitude 100 (ms):** Amplitude of the normal curve made with 100 successive beats. **Mode 100 (%):** Statistical mode of the normal curve made with 100 successive beats, expressed in percentage.

Consequently, in taller individuals, the dead space of the mask represents a relatively smaller proportion relative to their height.⁶

Our study focuses on short-term assessments conducted over durations of 5 min and 100 heartbeats. Consequently, our research lacks the prognostic capability inherent in 24-h follow-up studies, which examine broader outcomes such as morbidity or mortality. Additionally, our research has not delved into whether hypoxic and hypercapnic conditions induced by mask wearing exert any influence on blood pressure, a question addressed by findings from previous studies.^{4,14}

Conclusions

Upon removing facemasks during meditative rest, 86 % of subjects exhibited a clear sympathetic response for 5 min. 13 % showed consistent sympathetic responses throughout both phases of the study. Upon analyzing Ultra-Short-Term Cardiac Variability based on 100 beats, the significance of these observations became even more pronounced.

Our novel investigation, characterized by meticulous "RR" interval measurement over 4 min, reveals an increased parasympathetic predominance during facemask use at rest, influencing the autonomic loop regulation.

Conflicts of interest

None.

References

1. de Yzaguirre i Maura I, Zabala DD, Monaco M, Garcia JS, Miralles MR, Grazioli G. The use of facemasks and the impact on heart rate variability during baseline ECG. *Notes Sports Med.* 2023;58(219), 100416. <https://doi.org/10.1016/j.apunsm.2023.100416>, July–September.
2. F. Pifarri, D.D. Zabala, G. Grazioli, I. de Yzaguirre i Maura. COVID-19 and mask in sports. <https://doi.org/10.1016/j.apunsm.2020.06.002>.
3. De Yzaguirre I, Vives J, Gutiérrez JA, Brotons D, Tramullas A. Ergometry and climate change. *Notes. Medicina de l'Esport.* 2010;45:219–225.
4. I. De Yzaguirre Maura, Grazioli G, Mónica DF-C, Dulanto Zabala D, Sitges M, Gutierrez Rincon JA. Effect of rarefied air in a Mediterranean cave at cardiovascular level in humans». *Medicina De l'esport.* 2016;51:40–47. <https://raci.cat/index.php/Apunts/article/view/312642>.
5. I. De Yzaguirre Maura, Escoda J, Bosch J, Gutierrez Rincon J, Dulanto Zabala D, Segura Cardona R. Adaptation to the rarefied air of abysses and caves. A laboratory study. *Medicina De l'esport.* 2008;43:135–141.
6. I. de Yzaguirre et al. COVID-19: analysis of cavity air inspired through a mask, in competitive adolescent athletes. <https://doi.org/10.1016/j.apunsm.2021.100349>.
7. Reference of music used for meditative rest: <https://www.youtube.com/watch?v=kMrNsFwTXJQ>; <https://www.youtube.com/watch?v=BlxOU4wTsSU>.
8. Díturi J, Siddiqi F, Frisina R. Real-time heart rate variability analysis as a means of hypercapnia detection. *Undersea Hyperb Med.* 2019;46:503–507.
9. Baevsky, R. M. Chernikova, A. G. (2017). Heart rate variability analysis: physiological foundations and main methods. *Cardiometry.* 66–76. <https://doi.org/10.12710/cardiometry.2017.10.6676>.
10. Shaffer F, Ginsberg JP. An Overview of Heart Rate Variability Metrics and Norms. *Front Public Health.* 2017 Sep 28;5:258. <https://doi.org/10.3389/fpubh.2017.00258>. PMID: 29034226; PMCID: PMC5624990.
11. Nunan D, Sandercock GRH, Brodie EA. A quantitative systematic review of normal values for short term heart rate variability in healthy adults. *Pacing Clin Electrophysiol.* 2010;33:1407–1417.
12. Salahuddin L, Cho J, Jeong MG, Kim D. Ultra short term analysis of heart rate variability for monitoring mental stress in mobile settings. In: *Conf Proc IEEE Eng Med Biol Soc.* 2007. 2007:4656–4659.
13. Baek HJ, Cho CH, Cho J, Woo JM. Reliability of ultra-short-term analysis as a surrogate of standard 5-min analysis of heart rate variability. *Telemed JE Health.* 2015;21:404–414. <https://doi.org/10.1089/tmj.2014.0104>.
14. Brown S, Barnes MJ, Mundel T. Effects of hypoxia and hypercapnia on human HRV and respiratory sinus arrhythmia. *Acta Physiol Hung.* 2014;101:263–272. <https://doi.org/10.1556/APhysiol.101.2014.3.1>.
15. Tikhvinski SB, Khrushchev SV Children's Sports Medicine. Ed Meditsina Moscow. 1991:559–560.
16. Zemtsovski E.V., Baranovski A.L., Vasiliev. New method to record heart rate in athletes. *Theory Pract Phys Cult.* 1977, 6. p 1593–1599.